

# New Synthetic Surfactant – How and When?

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## Key Words

Pulmonary surfactant · Synthetic surfactant · Surfactant protein B · Surfactant protein C · Respiratory distress syndrome · Lung disease

## Abstract

Animal-derived surfactant preparations are very effective in the treatment of premature infants with respiratory distress syndrome but they are expensive to produce and supplies are limited. In order to widen the indications for surfactant treatment there is a need for synthetic preparations, which can be produced in large quantities and at a reasonable cost. However, development of clinically active synthetic surfactants has turned out to be more complicated than initially anticipated. The hydrophobic surfactant proteins, SP-B and SP-C, which are involved in the adsorption of surface-active lipids to the air-liquid interface of the alveoli and increase alveolar stability, are either too big to synthesize, structurally complex or unstable in pure form. A new generation of synthetic surfactants containing simplified phospholipid mixtures and small amounts of peptides replacing the hydrophobic proteins is currently under development and will in the near future be introduced into the market. However, more trials need to be performed before any conclusions can be drawn about the effectiveness of these synthetic surfactants in relation to natural animal-derived preparations.

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## Introduction

Surfactant deficiency in preterm babies causes respiratory distress syndrome (RDS). This disease can now be successfully treated by airway instillation of exogenous surfactants and the best results have been obtained with preparations purified from animal lungs, in some cases modified by addition of specific lipids. There has always been a concern about the potential risk of immunogenic and infectious complications using animal-derived surfactant preparations but after treatment of millions of infants no adverse effects of this nature have been described [1]. However, these surfactant preparations are expensive to produce and supplies are limited so there is a need to develop synthetic surfactants, which can be produced in large quantities at a reasonable cost.

The composition of pulmonary surfactant is very complex containing at least 50 different lipids [2] and four specific proteins – SP-A, SP-B, SP-C and SP-D [3]. The predominant surfactant component is the surface-active dipalmitoylphosphatidylcholine which is responsible for surface tension reduction to low values during expiration. Surfactant preparations purified from animal lungs by extraction with organic solvents contain this great variety of phospholipids and the two hydrophobic proteins SP-B and SP-C which are critical for the adsorption and spreading of the surfactant film at the air-liquid interface [3].

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## Synthesis of Surfactant Components

Development of clinically active synthetic surfactants has turned out to be more complicated than initially anticipated [4]. First, the complexity of the composition of phospholipids makes it difficult if not impossible to synthesize them all at a reasonable cost. Second, SP-B is too big and structurally complex to be synthesized by organic chemical methods and the expression of functionally active recombinant SP-B has not been reported. Third, SP-C is extremely hydrophobic and especially in pure form structurally unstable.

Incomplete knowledge of the function of some phospholipids in surfactant, in combination with limited commercial availability of many synthetic phospholipids, has resulted in the use of very simple phospholipid mixtures in synthetic surfactant preparations. Increased understanding of the molecular mechanism involved in formation and preservation of the surfactant film at the alveolar surface has led to the development of stable and rather simple peptides to replace native SP-B and SP-C.

## Peptides in Surfactants

Various molecules have been designed to substitute for the hydrophobic surfactant proteins SP-B and SP-C [5–20]. Recently, non-natural bioinspired structures based on poly-*N*-substituted glycines (peptoids) with  $\alpha$ -chiral side chains have been created to mimic both the SP-B fragment SP-B<sub>1–25</sub> [6] and the SP-C analogue SP-C(Leu) [7]. These non-natural molecules in a lipid mixture improve surface pressure-area isotherms, surfactant film morphology and dynamic adsorption, and decrease minimum and maximum surface tension during cycling in the pulsating bubble surfactometer. However, no data from *in vivo* studies with these synthetic surfactants have been published.

KL<sub>4</sub> is a 21-residue peptide which was designed to mimic the structure of SP-B [8] in particular SP-B(64–79) with the intermittent basic residues and the multiplicity of leucines in the hydrophobic stretches being near duplicates of the C-terminus of SP-B [9]. In contrast to the helix of SP-B(64–79) with its amphipathic surface, the KL<sub>4</sub> peptide presents its positive charges distributed over the entire helical circumference [10]. The surface structure of KL<sub>4</sub> thus differs from that of SP-B and segments thereof and also from SP-C with an  $\alpha$ -helix with exclusively unpolar residues [10].

Several peptides covering different parts of SP-B have been synthesized and their biophysical and physiological activities in different lipid mixtures have been evaluated *in vitro* and *in vivo*. N-terminal fragments of SP-B, especially residues 1–25, seem to mimic many of the *in vitro* activities of native SP-B [11] and a dimeric counterpart, dSP-B<sub>1–25</sub>, enhances surface properties compared to monomeric SP-B<sub>1–25</sub> [12]. A disulfide-linked construct based on the primary structures of the N- and C-terminal domains of SP-B (Mini-B) forms charged amphipathic helices and reproduces key *in vitro* and *in vivo* functions of full-length SP-B [13].

Synthetic surfactant based on recombinant SP-C but lacking the palmitoyl chains is highly effective at restoring lung function in surfactant-deficient animals [14]. Modification of the structure by replacing Cys4 and Cys5 with Phe, and Met32 with Ile gives a synthetic surfactant that improves lung function in premature newborn rabbits and lambs [15] as well as in animal models of acute lung injury [16]. Since the poly-valyl sequence in SP-C does not favor helix conformation, analogues with substitutions in this region have been designed. Replacement of the poly-valyl part of SP-C with a poly-leucyl stretch produces an analogue which forms an  $\alpha$ -helix [17–19]. However, this analogue has a strong tendency for peptide oligomerization. The problem was circumvented by synthesizing an SP-C analogue (SP-C33) with one positive charge in the N-terminal part of the  $\alpha$ -helical chain. SP-C33 in phospholipid mixtures can be suspended and administered at a concentration of 80 mg/ml. In preterm rabbit fetuses it increases lung compliance to levels similar to those obtained with commercially available modified natural surfactant preparations currently used for treatment of clinical RDS [20].

## Physiological Effects

The physiological effects of synthetic surfactant preparations have been assessed in both premature animals with surfactant deficiency [14, 15, 19–24] and in animals with acute respiratory distress syndrome (ARDS) [11, 13, 25–27]. Various animal models have been used but in contrast to natural surfactant preparations, synthetic surfactants seem to need positive end-expiratory pressure (PEEP) for surfactant response [15]. This indicates that natural surfactant preparations are more effective in stabilizing the airways. However, ventilation with PEEP is part of the routine management of patients with severe respiratory failure.

The efficacy of different surfactant preparations is difficult to compare in many studies using small groups of animals with large individual responses. In a recent study using 6 premature lambs with a gestational age of 135 days (term 145 days) in each treatment group, the conclusion was stated that lucinactant (Surfaxin) and poractant-alfa (Curosurf) produced similar improvements in gas exchange and lung mechanics even though 2 of the 6 animals did not respond to Surfaxin and the mean value of PaO<sub>2</sub> in this group was about 35% lower and the mean airway pressures higher than those for the Curosurf-treated lambs [23]. With small studies such as this, statistically significant differences in treatment efficacy will be virtually impossible to demonstrate. Thus, adequate sample sizes are needed to discover if different surfactant preparations have similar effects or they differ.

Two synthetic preparations have been used in clinical trials, recombinant SP-C (rSP-C) surfactant (Venticute) [28, 29] and Surfaxin [30–33]. Surfactant based on rSP-C improves lung function in different animal models [14–16, 27]. However, no results from clinical trials in preterm babies with RDS have been published and treatment with Venticute in patients with ARDS did not improve survival but had a positive effect on gas exchange [27, 28]. The other peptide-containing synthetic surfactant, Surfaxin, was given as prophylactic treatment to premature infants in two randomized clinical trials [30, 31]. In the study comparing Surfaxin and beractant (Survanta) the Surfaxin group was twice as large as the Survanta group [30]. The other study comparing Surfaxin and Curosurf was stopped when half the sample size had been recruited [31]. Larger studies are needed to conclude if Surfaxin is as effective as the natural surfactant preparations to prevent RDS in preterm babies. Surfaxin forms a gel that requires heating at 44°C for 15 min and subsequent shaking before tracheal administration [23, 30, 31]. This may

make it difficult to use Surfaxin as an emergency therapy. Furthermore, cooling of Surfaxin after the heating procedure to body or room temperature may increase the risk of gel formation which may result in plugging of the tracheal tube or the airways. Thus, the physical properties of surfactant preparations are important to avoid negative effects during treatment of patients.

### Concluding Remarks

Intensive research has provided increased understanding of molecular mechanisms of various surfactant components. These efforts have led to the development of peptides which may mimic the functions of the hydrophobic proteins SP-B and SP-C. New synthetic surfactant preparations based on these peptides and synthetic lipids will probably reach the market in the near future and may eventually replace natural surfactant preparations. In contrast to natural surfactant preparations, these synthetic surfactants seem to be physiologically active only during ventilation with PEEP but in patients with severe respiratory failure this type of ventilation is part of routine management. Thus, well-defined synthetic surfactants with good physiological activity and allowing production in large amounts at a reasonable cost are a prerequisite to use surfactant treatment for various lung diseases with inadequate surfactant function or as carrier for different drugs.

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